

MIND CONTROLLED ROBOT USING LDA CLASSIFICATION TECHNIQUE

ISSN (e) 2520-7393
 ISSN (p) 2521-5027
 Received on 10th May, 2018
 Revised on 29th June, 2018
 www.estirj.com

Muhammad Mansoor¹, Prof. Dr. Tariq Jamil Saifullah², Shahbaz Wahab³, Shaharyar Ahmed Abro⁴, Anjum Raza⁵

^{1,3,5}Department of Information Technology, Mehran University of Engineering & Technology, Jamshoro.

²Department of Computer Systems Engineering, Mehran University of Engineering & Technology, Jamshoro.

⁴Department of Computer Information Engineering, Mehran University of Engineering & Technology, Jamshoro.

Abstract: An ordinary robot those can be seen in market are helpful but still there is a great space available for further research. This paper is proposing a new type of robot which would be controlled by human. The robot being proposed would be completely controlled by human mind. Paper mainly proposes a methodology of controlling of robot's motion by the interface of brain and computer system that would be embedded in robot. Intel Computer stick is proposed to be used to achieve the embedded system. Signal classification scheme is recommended, and those signals are captured using EPOC nerve gear. The classifier being used for the purpose is Linear Discriminate Analysis (LDA). The results being achieved by the methodology proved to be efficient enough to be deployed in daily lives of human.

Keywords: Mind-Controlled; EPOC; Brain Computer Interface (BCI), Filters, Linear Discriminate Analysis (LDA); Mean; Co-Variance.

1. Introduction

Interface between brain and computer is a system where electrodes are attached to the scalp of user and that is how a direct way is created between brain and computer. A human brain creates different type of signals while thinking process. So these signals represent the set of instructions a person wants system to implement. Those signals or set of instructions are noted from the scalp through Electroencephalography (EEG).

A well-defined induction is proposed by many researchers. And state of the art induction technique of electrodes over the scalp is presented in figure 1 [3]. Electrodes being recommended by researchers are of Silver Chloride [4].

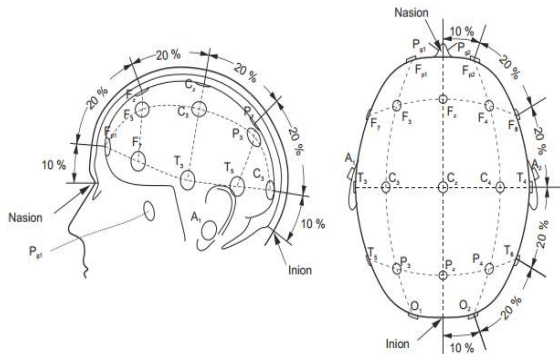


Figure 1 Induction of Electrodes over Scalp

For recording some accurate signal researchers have proposed an impedance of 1 to 10 [5], for which we can also be needed to use some type of gel so that we can keep impedance under our range.

Signals being acquired from the scalp are of different

ranges. So, in order to classify the signal frequency should be in users control. Five different frequency ranges are observed which are Gamma, Beta, Alpha, Theta and Gamma.

Table 1 discusses about different frequency bands those are acquired by the scalp for signals of instruction to the robot. These different bands hold different information regarding the motion being conveyed by the user.

Table 1 Different frequency Bands

Frequency Band	Band Range	Information	Reference
Delta	Below 4Hz	Very low frequency therefore confusion occurs as muscles also produce low frequency in normal.	[6]
Theta	Between 4Hz to 7Hz	Are being observed in meditative concentration.	[7-9]
Alpha	Between 8Hz to 12Hz	Band is more related to the visual information or instruction.	[10-13]
Beta	Between 12Hz to 30Hz	Only produced while muscles produce greater motion.	[14]
Gamma	Between 30to 100Hz	Strongest among all, there for very less chance of confusion.	[15]

Emotiv EPOC is utilized for acquiring signals. Figure 2 illustrates the model of EPOC and shows its positions of the EEG wet electrodes. The specifications include wireless transmission of signals via Bluetooth 2.0. The device is used as a head set and electrodes can easily be located on the scalp.

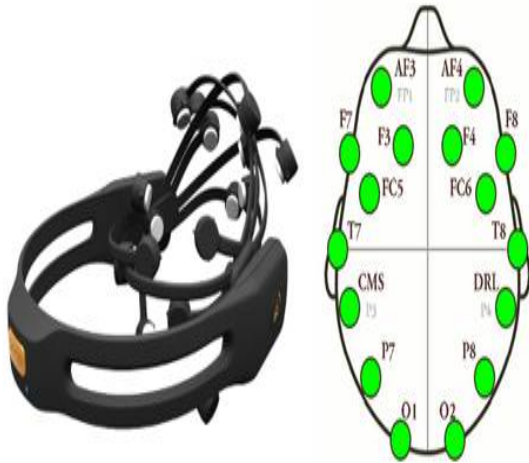


Figure 2 Headset as Hard (Left), Placement of wet electrodes (Right)

2. Methodology

The proposed methodology includes three steps which are as follows,

- Signal Acquisition
- Feature Extraction
- Classification

Further Figure 3 summarizes the overall methodology steps.

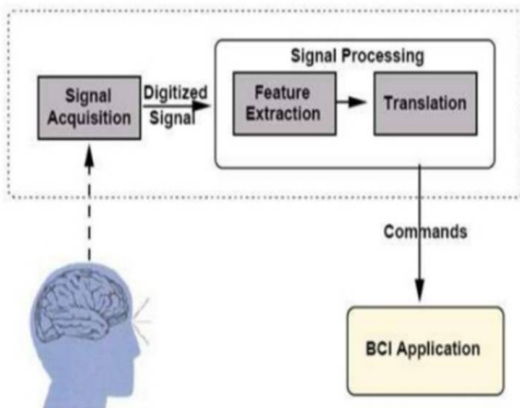


Figure 3. Overall Methodology steps

2.1 Signal Acquisition

Signals are acquired by the scalp through the help of electrodes placement over scalp. Emotive EPOC is a device that is being utilized for acquiring of signals. The

placement of respective electrodes is discussed before. A timing scheme is followed for signal acquisition which is showed in figure 4.

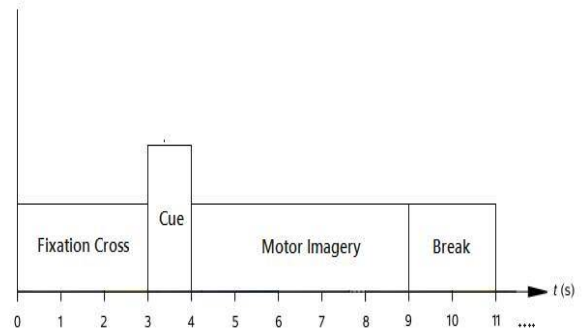


Figure 4. Timing scheme followed for acquisition of BCI data

So, the output of the first step would be signal where signal is generated using whole system.

2.2 Features Extraction

After the process of signal acquisition, the signals are recorded in the dataset. Feature Extraction is one of the most important part of the proposed methodology. As these features would be used for making feature extraction and after that those feature vectors would be used for the purpose of classification. Now the recorded dataset would be used for feature extraction. Four different filters have been utilized for this purpose. The filters proposed are Chebyshev filter, Butterworth filter, Common Spatial filter and Logarithmic Band Power. The Discrete Continuous Fourier transform of the signals in dataset is taken and the output coefficients are fed into the named filters. The coefficients of the signals would be frequency domain.

The bellow equation illustrates the formulation used for deploying Chebyshev filter. Chebyshev filter gives the features lying near its cut-off.

$$G_n(\omega) = |H_n(j\omega)| = \frac{1}{\sqrt{1 + \epsilon^2 T_n^2\left(\frac{\omega}{\omega_0}\right)}}$$

Where,

$$\epsilon = \sqrt{10^{0.1\delta} - 1}$$

w= The frequency being input

w0= The cut-off frequency

Below figure illustrates the recorded response of implemented Chebyshev filter for feature extraction. It depicts how different orders can be used for the extraction of features. The Chebyshev filter used in the proposed methodology is of order 2 as it holds lets lobes in comparison to others.

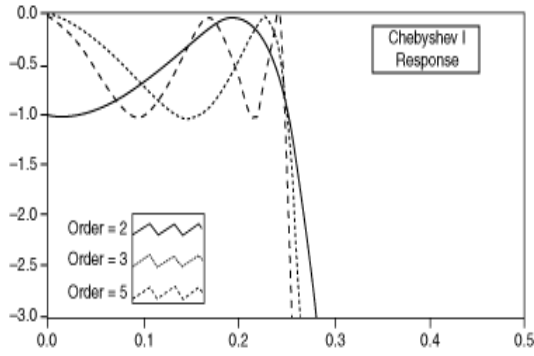


Figure 5. Chebyshev Response

Second filter been used is Butterworth filter. The equation being used for this purpose is shown below. Where w is the frequency coefficient received after discrete continuous transform.

$$G(\omega) = \sqrt{\frac{1}{1 + \omega^{2n}}}$$

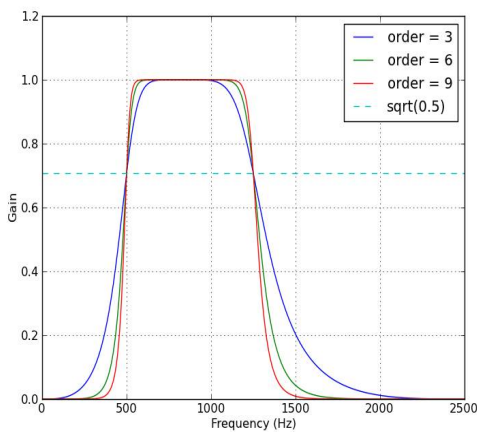


Figure 6 Butterworth Filter

Above is the response of Butterworth filter. As can be seen that Butterworth filter gives flat amplitude response. This filter can be used for comparison of amplitude of different signals. So amplitude detection can easily be done by it.

Surface Laplacian is used to increase the variance between different classes of signals. The major feature by Surface Laplacian is variance which contributes towards classification.

Logarithmic Band Power is used to extract power feature from BCI signals. The power of the signals would vary as per instruction. So in proposed methodology this is the strongest feature being used for the purpose of classification. Below is the equation being used for this purpose.

$$u(x) = \log(1+x^2)$$

Further logarithmic band power is followed by feature aggregator which concatenates the features into single vector. And the Feature Vector is obtained from the described process.

2.3 Classification

After feature extraction classification between different signals needs to be performed so that different motions can be classified. In proposed methodology Linear Discriminate Analysis (LDA) is being used as a classifier.

LDA is one of the most Robust classifier available, as it reduces the complexity and dimensionality. LDA is a binary classifier which is used for classification of two classes. The output of the LDA mainly classifies under mean and variance of different classes. And same stands in the proposed scheme, As variance is one of the strongest feature being extracted in our methodology. Here LDA would be classifying between right and left motion. Figure 7 discusses the flow under which mechanism LDA works, and classifies different classes.

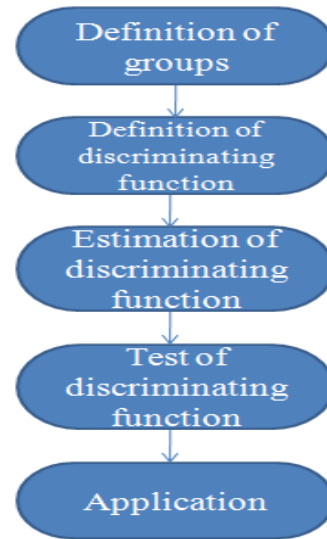


Figure 7 LDA Scheme

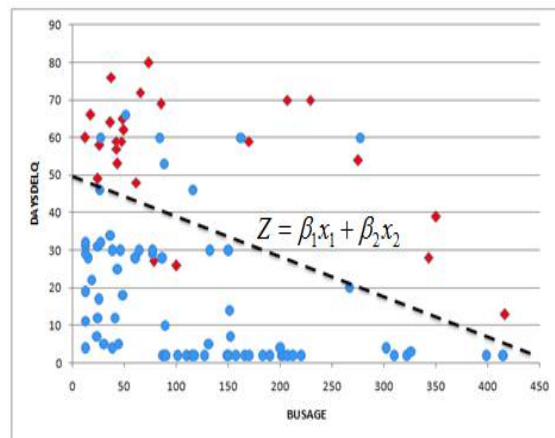


Figure 8. LDA scatter plot of Feature Separation

Further figure 8 shows how LDA classifier classifies the features. Two different type of features are plotted and how through linear regression the classifier has separated the feature clusters.

3. Result

Results are being carried out using LDA. The table 2 shows how well LDA has classified two different decisions. The main parameters used for the comparison are Mean of the feature vectors and covariance between feature vectors. Mean and variance were one of the strongest features which were extracted using different filters as discussed in the methodology. The difference between mean and covariance is high enough which clearly depicts that the classification is done well.

Table 2 Comparative results

Class (DEFAULT)	Count	Probability	Statistics	BUSAGE	DELQDAYS
N	$n_1=75$	$p(c_1)=0.75$	Means Vector (μ)	116.23	16.89
			Covariance Matrix (C)	$\begin{bmatrix} 9323 & -607 \\ -607 & 333 \end{bmatrix}$	
Y	$n_2=25$	$p(c_2)=0.25$	Means Vector (μ)	115.04	55.32
			Covariance Matrix (C)	$\begin{bmatrix} 14009 & -1053 \\ -1053 & 287 \end{bmatrix}$	

4. Conclusion

A Methodology for mind-controlled robot is being proposed in the paper. Which includes signal acquisition from scalp than feature extraction from those signals and lastly the classification part. The classification results clearly depict that the proposed methodology is highly efficient to be used for the betterment of human life. And the features those are proposed for the classification of signals for the purpose are mean and variance as proved by the results.

Acknowledgment

Authors are indebted to acknowledge with thanks to Prof. Dr. Zubair Ahmed Memon, Director, Institute of Information & Communication Technologies, and supervisor Prof. Dr. Tariq Jamil Saifullah Khanzada for their moral support and Mehran University of Engineering & Technology, Jamshoro, Pakistan, for providing necessary facilities to complete this research work and valuable suggestions of anonymous reviewers for improving the readability of this paper.

References

- [1]. Chu, Narisa NY. "Surprising Prevalence of Electroencephalogram Brain-Computer Interface to Internet of Things [Future Directions]." *IEEE Consumer Electronics Magazine* 6.2 (2017): 31-39.
- [2]. Brandman, David M., et al. "Rapid calibration of an intracortical brain-computer interface for people with tetraplegia." *Journal of neural engineering* 15.2 (2018): 026007.
- [3]. A.P, J. (2005). The functional significance of mu rhythms. *Brain Res. Rev.* 57-68.
- [4]. Aftanas, L., & Golocheikine, S. (2001). Human anterior and frontal midline theta and lower alpha reflect emotionally positive state and internalized attention: high resolution EEG investigation of meditation. *Neurosci Lett*, 57-60.
- [5]. Diez, Pablo F., et al. "Commanding a robotic wheelchair with a high-frequency steady-state visual evoked potential based brain-computer interface." *Medical engineering & physics* 35.8 (2016): 1155-1164.
- [6]. Chien, Y. Y. *et al.* Polychromatic SSVEP stimuli with subtle flickering adapted to brain-display interactions. *J. Neural Eng.* **14**, 016018 (2017).
- [7]. Han, Jae Joon, et al. "Increased parietal circuit-breaker activity in delta frequency band and abnormal delta/theta band connectivity in salience network in hyperacusis subjects." *PloS one* 13.1 (2018): e0191858.
- [8]. Brown, P., Salenius, S., Rothwell, J., & Hari, R. (1998). Cortical correlate of the piper rhythm in humans. *Neurophysiol*, 2911-2917.
- [9]. Fernández T1, H. T. (1995). EEG activation patterns during the performance of tasks involving different components of mental calculation. *Electroencephalogr Clin Neurophysiol*, 175-182.
- [10]. Fonseca, C., Cunha, J., Martins, R., Ferreira, V., de Sa, J., Barbosa, M., & Silva, d. (2007). A novel dry active electrode for EEG recording. *IEEE Trans Biomed Eng.* 162-165.
- [11]. Acqualagna L., Blankertz B. (2015). Neural correlates of relevant stimuli processing for brain computer interfaces, in *Engineering in Medicine and Biology Society (EMBC), 2015 37th Annual International Conference of the IEEE (Milano: IEEE;)*.
- [12]. Pfurtscheller, G., & Neuper, C. (2001). Motor imagery and direct brain-computer communication. *Proc.IEEE*, 1123-1134.
- [13]. Pfurtscheller, G., Brunner, C., Schlögl, A., & Lopes da Silva, F. M.-t.-1. (2006). Murhythm (de)synchronization and EEG single-trial classification of different motor imagery tasks. *Neuroimage* , 153-159.
- [14]. Sinclair, C., Gasper, M., Blum, A., & Neurophysiology, B. E. (2007). *The Clinical Neurophysiology Primer* . 3-18.
- [15]. Usakli. (2010). Improvement of EEG signal acquisition: An electrical aspect for state of the art of front end. *Computational Intelligence and Neuroscience*, 7.
- [16]. Venables, L., & Fairclough, S. (2009). The influence of performance feedback on goal-setting and mental effort regulation. *Motiv. Emotion* , 63-74.
- [17]. Akram S., Presacco A., Simon J. Z., Shamma S. A., Babadi B. (2016). Robust decoding of selective auditory attention from MEG in a competing-speaker environment via state-space modeling. *Neuroimage* 124, 906-917.

About Authors



Muhammad Mansoor completed B.E in Computer Systems Engineering from Mehran University of Engineering & Technology, Jamshoro, Pakistan. Currently, He is enrolled in Master of Engineering from Institute of Information & Communication Technology, (IICT), and going to be finished. He has been working as a designer ,developer and technical writer in a Software House. His research interests are Networking, design and development and Artificial Intelligence.



Shahbaz Wahab completed his B.E in Computer Systems Engineering from Mehran University of Engineering & Technology, Jamshoro, Pakistan. He is currently enrolled in Master of Engineering from Institute of Information & Communication Technology, (IICT), and going to be finished. He has been working as a designer ,developer and Computer Networks. His research interests are Networking, design & development and Artificial Intelligence.